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Title: In vivo human brain imaging at 0.2 T with a whole body fast field-cycling system
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Abstract: **Purpose**
Fast Field-Cycling (FFC) MRI systems obtain unique dispersive contrast through their ability to alter the main magnetic field strength B_0 during the pulse sequence. In a typical pulse sequence, the field strength is changed from the polarization field, B_{0p} , to the evolution field, B_{0e} , at which relaxation effects of interest occur, before returning to the detection field, B_{0d} . Switching the field requires novel magnets, power supplies and ancillary devices.

Methods
The literature contains several examples of FFC apparatus. In general they are home-built systems with dual-magnet designs, in which a stable and homogeneous field from one magnet (superconducting or resistive) providing B_{0d} is offset by a secondary electromagnet to generate B_{0e} . In contrast, this magnet follows a single-magnet design with rigorous requirements for field homogeneity and stability.

The magnet consists of three co-wound copper coils on a cylindrical former embedded in epoxy resin (Tesla Engineering Ltd, Storrington, UK). It is 2080 mm in length and 500 mm in bore, make it suitable for human subjects. A current of 650 A (in each of three circuits) generates a field strength of 0.2 T. This current is provided by a specially-made bank of high-power gradient amplifiers (International Electric Co. Oy, Helsinki, Finland) with a custom control system.

Results
We have obtained 64 x64 pixel transaxial spin-echo FFC images of the brain of a healthy volunteer using acquisition parameters:
field of view 300 mm , slice thickness 10 mm, TE 10 ms, TR 1500 ms, field ramp time 20 ms, polarization time 500 ms, $B_{0p} = B_{0e} = B_{0d} = 196$ mT (8.34 MHz proton frequency)

Outlook
We intend to demonstrate the novel contrast that can be obtained, in vivo, by selecting B_{0e} values in a range of low 10's mT and ultra low sub mT regions.

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